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TITLE OF THE INVENTION

Living Body Photometric Apparatus

FIELD OF THE INVENTION

The present invention relates to a living body
5 photometric apparatus, which measures information
inside a living body by making use of light beams and
more specifically, relates to a living body photometric
apparatus, which can specify accurately and easily a
reactive portion inside the living body when a task load
10 is given to the living body.

CONVENTIONAL ART

A living body photometric apparatus is an
apparatus in which light beams having wavelength from
visible region to infrared region are irradiated to a
15 living body and reflected or scattered light beams
inside the living body are detected so as to measure
information inside the living body, and with which blood
circulation and blood circulation dynamics inside the
living body, moreover, variation in time of light
20 absorption materials in blood such as hemoglobin can
be easily measured with less restriction to a subject
and without giving any harms to the subject. Thus
clinical application of the living body photometric
apparatus is expected.

25 In the living body photometric apparatus, the
measurement result is displayed such as in a graph
representing hemoglobin density variation in time at

a measurement position (time course representation) and in a contour imaging (topography) of a spatial distribution variation of hemoglobin at a measurement region. Further, the measurement result is displayed 5 as an image in a color phase such as red and blue assigned to spatial distribution of hemoglobin and variation in time thereof.

Examples of clinical applications of the living body photometric apparatus are such as local focus 10 identification of epilepsy and language area region identification examination as presurgical examination of epilepsy therapy. The language area region identification examination is a very important examination suppressing damage low for brain function 15 tissue at the time when removing the local focus portion of epilepsy and is required to correctly specify the region.

The language area region identification examination by making use of the living body photometric apparatus is, for example, disclosed in E. Watanabe et 20 al., "Non-invasive assessment of language dominance with near-infrared spectroscopic mapping" Neuroscience Letters 256 (1998) 49-52, in which hemoglobin variation signals are measured from a 25 plurality of positions for each of the right and left temporal lobes while giving a subject language stimulus loads, the obtained plurality of hemoglobin variation

signals are added and averaged for every right and left temporal lobes and through comparison of these averaged values the language area region is identified.

Further, such as the present applicants are now 5 developing a living body photometric apparatus, which improves convenience in living body photometry and objectivity in measurement and is suitable for the language area region identification (see JP 11-311599 A and WO 02/32317 A1)

10 As has been explained above, for identification of an active region in the brain such as the language area region identification, it is important to diagnose a correct position thereof, and the living body photometric apparatus is required to provide correct 15 information and information facilitating diagnosis.

However, when performing examination for specifying the small language area region of about 3 cm x 3 cm, since in the hemoglobin variation signals measured other signals than activation signals in the 20 brain brought about by a load for the language area region identification, for example, signals due to hand motion for writing letters and further, signals due to such as the sense of sight and the sense of hearing are contained, the diagnosis accuracy of the method of 25 specifying the active portion brought about by the loading through average value comparison of the signals of right and left temporal lobes is not high and remains

in about 60 %. For this reason, in the region specifying examination by making use of the living body photometric apparatus, the apparatus is desired to be able to specify a small region as well as to be able to improve 5 diagnosis accuracy.

Further, with the conventional display method in the living body photometric apparatus such as the time course representation of hemoglobin variation signals for every measurement channel and the topography 10 representation, it was sometimes difficult to easily grasp a specific active region.

Accordingly, an object of the present invention is to provide a living body photometric apparatus, which can accurately specify an objective small active region 15 in a brain from hemoglobin variation signals measured.

SUMMARY OF THE INVENTION

In order to achieve the above object, the present invention is characterized in that a signal processing portion of the living body photometric apparatus is 20 added of a function, which performs a principal component analysis for signals measured. The principal component analysis function is understood to be able to extract from the signals measured only signals corresponding to the loaded task. Thereby, an apparatus, 25 which permits to effectively compare interregional signal intensity and to accurately identify an active portion in the brain in a clinical examination

application such as the language area region identification.

Namely, the living body photometric apparatus according to the present invention comprises a light measurement portion which measures intensity of passing light at a plurality of measurement points of a subject and outputs signals corresponding to intensity of passing light for every measurement point as measurement data for every measurement channel, a signal processing portion which processes the measurement data output from the light measurement portion and images a living body reaction when a predetermined task is given to the subject and an input and output portion which displays a processed result of the signal processing portion as well as sends a command necessary for a processing in the signal processing portion, characterized in that the signal processing portion includes means for performing a principal component analysis for the measurement data and for extracting a representative signal which most reflects the living body reaction when the task is given.

Specifically, the signal processing portion performs a principal component analysis for the measured data, calculates not less than one representative signal and weight of the representative signal for every measurement channel, correlates the

representative signal with a referential response signal representing a passing light pattern when the task is given and extracts a representative signal reflecting most the living body reaction when the task 5 is given among the representative signals as a task related signal.

According to the living body photometric apparatus of the present invention, since the representative signal reflecting most of the living body reaction when 10 the task is given can be extracted as the task related signal, through comparison of the weight of the task related signal for every measurement channel, namely comparison of abundance frequency, an active portion which reacts most with respect to the task (language 15 area when the task is language stimulus) can be accurately specified.

The present invention further provides a living body photometric apparatus with an improved display function. Namely, the living body photometric apparatus 20 according to the present invention is characterized in that the input and output portion is adapted to display a waveform of the representative signal calculated through the principal component analysis in the signal processing portion and the weight of the representative signal for every measurement channel. Further, the living body photometric apparatus according to the present invention is characterized in that the 25

calculated result of the correlation between the representative signal and the referential response signal is displayed together with the waveform of the representative signal.

5 According to the present living body photometric apparatus, from a screen on which the waveform of the representative signal is displayed, a user can discriminate among the representative signals the task related signal which is a representative signal showing
10 the highest correlation with the referential response signal, and further, from the weight of the task related signal for each measurement channel, the user can discriminate a most reactive portion (a concerned measurement channel) to the task.

15 In a further preferable living body photometric apparatus according to the present invention, the signal processing portion receives a condition for the task from the input and output portion and prepares a referential response signal depending on the condition.

20 According to the present living body photometric apparatus, since a referential response signal of a suitable reaction pattern depending on the task can be used, correctness when extracting the task related signal is improved.

25 In a still further preferable living body photometric apparatus according to the present invention, the signal processing portion divides the

measurement channels into a plurality of groups, calculates average values of the weights of each measurement channel for every groups with respect to the representative signal selected as the task related 5 signal and further calculates from the average values dominance of the response with regard to the task in the groups thereby to display the same.

BRIEF DESCRIPTION OF THE DRAWINGS

Fig.1 is a block diagram showing a schematic entire 10 structure of a living body photometric apparatus according to the present invention;

Fig. 2 is a flowchart of language area region identification diagnosis performed by the living body photometric apparatus according to the present 15 invention;

Fig. 3 is a view showing an attachment state of a probe to a subject when the measurement object is a head;

Fig.4 is a view showing an example in which a 20 measurement result of hemoglobin variation signal in response to a language stimulus loading is displayed on a screen;

Fig.5 is a view for explaining a principal component analysis performed for hemoglobin variation 25 signal measured;

Fig.6 is a view showing an example in which a result of the principal component analysis for the hemoglobin

variation signal is displayed on the screen;

Fig.7 is a view showing an example of a screen for preparing a referential response signal which is used for analyzing the hemoglobin variation signal; and

5 Fig.8 is a flowchart of dominance hemisphere identification performed by the living body photometric apparatus according to the present invention.

DETAILED DESCRIPTION OF THE EMBODIMENT

Herein below an embodiment of the present invention will be explained in detail. In the explanation below, as an object of light measurement, amount of hemoglobin (including oxy hemoglobin, deoxy hemoglobin and total hemoglobin) in a living body is referred to, however, in the living body photometric apparatus according to the present invention, substances such as cytochrome other than the hemoglobin which absorb light beams of near infrared region can be used as the measurement object.

Fig.1 is a block diagram showing a schematic entire structure of a living body photometric apparatus according to the present invention. The living body photometric apparatus is provided with a light source 10 which irradiates near infrared light beams to a living body, an optical measurement portion 20 which measures light passed through the living body and converts the same into an electrical signal and a signal processing portion 30 which calculates living body

information, more specifically, hemoglobin density variation in blood at a measurement portion based on the signals from the optical measurement portion 20 and displays the result. Further, in order to contact an 5 end of an optical fiber to a measurement position of a subject for transmitting light beams from the light source 10 as well as to contact an end of another optical fiber to a measurement position of the subject for detecting light beams passed (including scattered) 10 inside the living body and for transmitting the same to the optical measurement portion 20, the living body photometric apparatus is provided with an attachment member 40 for securing the ends of these optical fibers at predetermined positions. Herein below, the 15 attachment member and the end portions of the optical fibers secured to the attachment member will be called inclusively as a probe 300.

The light source 10 is constituted by semiconductor lasers 11, which respectively emit light 20 beams having a plurality of wavelengths (synonym of frequency) in a region from visible to near infrared, for example, wavelengths of 780nm and 830nm, a plurality of optical modules 12 provided with modulators for modulating the light beams of the two wavelengths into 25 a plurality of different frequencies and a plurality of irradiation use optical fibers 13, which guide the light beams output from the optical modules 12 to the

probe. The light beams of the two frequencies irradiated from the semiconductor lasers 11 are mixed and input in respective optical modules 12 wherein the same are modulated in different frequencies in every optical 5 modules, and the modulated light beams of the two frequencies are irradiated to the respective examination portions of the subject via the respective irradiation use optical fibers.

The optical measurement portion 20 is connected 10 to detection use optical fibers 21 and is constituted by photo-electric conversion elements such as photo diodes 22 which convert the amount of the light beams transmitted by the respective detection use optical fibers 21 to respective corresponding electrical 15 signals, lock-in amplifier modules 23 to which the electrical signals from the photo diodes 22 are input and from which selectively output signals corresponding to respective irradiation positions and detection positions as well as the frequencies and an A/D 20 converter 24 which A/D converts the signals output from the lock-in amplifier modules 23. Number of lock-in amplifier modules 23 to be provided is at least the same number of the signals to be measured.

The probe 300 is constituted in such a manner that 25 a matrix of proper size such as 3x3 and 4x4 with a predetermined pitch is formed on the attachment member 40 and the ends of the irradiation use optical fibers

and the ends of the detection use optical fibers alternatively disposed thereon by making use of a securing use socket.

The light beams detected by the detection use optical fibers in the living body photometric apparatus are mixture of a plurality of light beams having different frequencies, which are respectively irradiated from a plurality of adjacent irradiation use optical fibers and passed inside the living body. The lock-in amplifier modules 23 selectively detect these pluralities of signals having different frequencies with reference to the irradiation positions, irradiation frequencies and detection positions thereof. Thereby, information inside the living body is detected at measurement points determined by points between the end positions of the irradiation use optical fibers and the end position of the detection use optical fibers, more specifically, the intermediate points thereof.

These measurement points correspond to the number of channels detected by the lock-in amplifier modules 23, for example, in a case of a probe having 3x3 matrix, the number of measurement points between the irradiation positions and the detection positions is 12, thus a light measurement of 12 channels can be performed.

The signal processing portion 30 is connected to

the optical measurement portion 20 via a control portion (centralized processing unit: CPU) 31 for controlling the entirety of the apparatus, processes the voltage signals (digital signals) sent from the optical measurement portion 20 and performs conversion thereof into signals representing living body information, more specifically, conversion into hemoglobin variation signals representing hemoglobin density and variation thereof in time at the measurement portions and preparation of data for topography image. Other than the above referred to image preparation function, the signal processing portion 30 includes such as a function of extracting from the hemoglobin variation signals measured at the respective measurement channels signals (task related signals) representing a feature of a task (load) given to the subject at the time of the measurement and a function of calculating based on the task related signals the most reactive measurement portion (channel) with respect to the task. In order to perform these functions, the signal processing portion 30 is provided with an arithmetic unit.

The CPU 31 controls such as operations of light beam irradiation and detection, an application timing of the load (stimulus), processing including the analysis of the measured signals and preparation of images and display thereof. For this purpose a variety of softwares are assembled into the CPU 31. Further, the

arithmetic function of the signal processing portion can be borne by the CPU 31.

The living body photometric apparatus is further provided with a memory portion 32 in which digital 5 signals sent from the optical measurement portion 20 and data of after signal processing are stored and an input and output portion 33 which displays the processed result in the signal processing portion 30 as well as permits to input necessary instructions for the 10 measurement and signal processing. More specifically, the input and output portion 33 is provided with a input manipulation board including on/off switches, key board and mouse and a display unit of such as CRT and liquid crystal.

15 In the thus constituted living body photometric apparatus, the light measurement is performed in such a manner that the light beams modulated in different frequencies are irradiated from the probe 300 attached to the living body through the irradiation use optical 20 fibers 13, the light beams passed through the living body and detected by the detection use optical fibers 21 are respectively converted into electrical signals, which are detected for every measurement point at an intermediate point between respective irradiation 25 positions and detection positions and hemoglobin variation signals are obtained by converting the electrical signals into variation in time of the

hemoglobin densities in blood at measurement portions. The hemoglobin variation signals measured at the respective measurement points are subjected to a variety of analysis in the signal processing portion 5 and these analysis results are displayed on the monitor screen in the input and output portion 33.

Now, an example of sequences for specifying a reactive portion of the living body in response to a predetermined task in the above explained living body 10 photometric apparatus will be explained with reference to the flowchart in Fig.2. The following explanation is a sequence effective for identifying a language area region in presurgical examination for epilepsy.

At first the probe is attached to the right and 15 left temporal lobes of the subject (step 201). Fig.3 shows the probe attached. As shown in the drawing, in the present embodiment, the top ends of the irradiation use optical fibers and the top ends of the detection use optical fibers are arranged in a matrix of 3x3. As 20 has been explained previously, since the measurement points are located at the intermediate points between the arranged points of the irradiation use optical fibers and the detection use optical fibers, the number of measurement points, namely, the number of channels 25 in the probe formed in the matrix of 3x3 of the present embodiment is 12. Probes 301 and 302, each having 12 channel measurement points, are attached respectively

to the right and left temporal lobes. Further, in Fig. 3, for example, 9 total optical fibers including 4 irradiation use optical fibers and 5 detection use optical fibers are arranged at crossing points of the 5 matrix in such a manner to sandwich the positions indicated by measurement channel numbers. Accordingly, in the case of the present embodiment in which the probe is attached to the right and left temporal lobes, 8 of the optical modules 12 and 8 of the irradiation use 10 optical fibers 13 in the light source portion 10 and 10 of the detection use optical fibers 21 and 10 of photo diodes in the optical measurement portion 20 are required.

After completing the attachment of the probes 301 and 302 to the living body, the measurement is performed 15 (step 202). The measurement begins to turn on a measurement switch provided at the input and output portion 33. When turning on the measurement switch, the semiconductor lasers 11 in the light source 10 are 20 oscillated and emit light beams having different wavelengths of 780nm and 830 nm, and the light beams having the two wavelengths are mixed and input into optical modules 12a, ··· 12h, the two light beams having 780nm and 830nm input into respective optical modules. 25 are modulated into different frequencies for every module by a modulator in respective optical modules. These modulated light beams are guided to the probes

301 and 302 via the irradiation use optical fibers 13a, ··· 13h and are irradiated onto the right and left temporal lobes. The irradiated light beams pass through the skin and the skull and after repeating passing and 5 scattering of the light beams through the fine blood vessels and tissues in the brain, the light beams input into probe side openings for the detection use optical fibers 21a, ··· 21j. Further, since the light absorbance characteristics of oxy hemoglobin and deoxy hemoglobin 10 are different depending on the wavelength thereof irradiated from the irradiation use optical fibers, the light amount input from the detection use optical fibers differs depending on amount of hemoglobin in blood vessels at the detection portions. The light beams input 15 into the detection use optical fibers 21a, ··· 21j are respectively converted into electrical signals by the photo diodes 22a, ··· 22j and these electrical signals are discriminated according to the frequency thereof by the lock-in amplifier modules 23. Since the frequency of 20 the light beams irradiated from the irradiation use optical fibers corresponds to the positions of the optical fibers and the positional relationship between the detection use optical fibers and the irradiation use optical fibers are determined, the frequencies of 25 the signals discriminated at the lock-in amplifier modules 23 and the measurement points are coordinated. Then the signals output from the lock-in amplifier

modules 23 are converted into digital signals by the A/D converter 24 and output to the signal processing portion 30 in which signal processing such as for analysis and image display is performed.

5 The above measurement operation is performed while giving a predetermined task (stimulation) to the subject and the hemoglobin variation signals are obtained from the subject. In the above example, since 10 an identification of the language area is an object, stimulations for activating the language area such as a game of making word chains and writing of words having a same pronunciation are given as the task. The task can be replaced by other stimulation to five senses to 15 the living body such as visual stimulation, olfactory stimulation, auditory stimulation and pain stimulation depending on the diagnosis object. Then the measurement is performed by combining an application period (loading period) of the language stimulation and rest period (no load period) as a set and by repeating the 20 set in plurality of times.

 The hemoglobin signals appear as difference signals between the signals measured under a condition when no load (stimulation) is given to the brain of the subject and the signals measured after applying a load 25 and one set of difference signals is obtained from the respective channel 1 through 24 in the right and left probes 301 and 302 at the same time and is displayed.

When the language stimulation is repeated, namely, a plurality set of hemoglobin variation signals are obtained in a time course, the latest information or averaging after adding the plurality set of signals for 5 respective channels is displayed.

Fig.4 shows an example of displayed images on the monitor. As shown in the drawing, the hemoglobin variation signal 401 is displayed in a time course graph for every channel wherein abscissa is time axis and 10 ordinate is hemoglobin density. In the graph, a stimulation start point (time) 402 and a stimulation end point (time) 403 are indicated on the ordinate. Further, on the monitor screen a variety of command 15 input buttons such as "Calc PCA" 404 and "Reference Graph" 405 are provided in order to permit an operator to send a subsequent processing command to the control portion 31 and the signal processing portion 30. These input buttons are always displayed on the following display screens.

20 The signal processing portion 30 performs a principal component analysis processing for the hemoglobin variation signals of the respective channels measured in step 202. The principal component analysis processing is a known method in the field of mathematics 25 and in the present embodiment, a pattern having high abundance frequency with respect to energy is extracted among the plurality of detected signals. In other words,

some of representative signals having a contribution rate more than a predetermined contribution rate for the 24 channel hemoglobin signals measured are calculated (step 203). The principal component analysis 5 processing is executed by clicking the "Calc PCA" button 404 on the screen in Fig.4. The principal component analysis is a method of converting high dimensional data into further low dimensional data without losing information as much as possible and in the present 10 embodiment, as shown in Fig.5, with regard to a plurality of measured data of hemoglobin variation signals defined by axes of time and channel number, the dimension (24 channels) of the channel axis is compacted and is converted to data having further less channels. 15 Further, when "Calc PCA" button 404 is clicked, the display screen is changed over from one shown in Fig.4 to one shown in Fig.6.

The contribution rate is an index showing how much a principal component (representative signal) 20 extracted via the principal component analysis expresses the feature contained in the measured data and can be determined by calculating "a ratio of variance of the principal component occupying in the total variance" in the principal component analysis. 25 In the present embodiment, a representative signal having, for example, more than 90% contribution rate is calculated.

An example of images displaying the result of the principal component analysis is shown in Fig. 6. As shown in the drawing, in the present embodiment, two kinds of signals 601 and 602 are extracted and displayed as 5 the representative signals. Since these two kinds of signals express more than 90% measurement data for all the channels, a third signal 603 is not calculated.

When calculating the representative signals by compacting the measured data with regard to the channel 10 axis in the principal component analysis, coupling coefficients to be multiplied to the respective channels are calculated. These coupling coefficients are weights in the respective channels for the representative signals, namely, correspond to the 15 abundance frequencies. Weights 607 and 608 for the respective channels calculated with respect to the representative signals 601 and 602 are, for example, shown in a bar graph in which abscissa is the channel number and ordinate is the weight and are displayed 20 adjacent to the representative signals. A relationship between actual signals measured, representative signals and the weights will be explained, for example, with reference to a eighth channel, in that an added value of a value determined by multiplying the 25 representative signal 601 with the weight for the eighth channel adjacent to the representative signal 601 and a value determined by multiplying the representative

signal 602 with the weight for the eighth channel adjacent the representative signal 602 is substantially the same as the actually measured value for the eighth channel. Further, the weights displayed in the bar graph 5 are effectively used by the operator for identifying the most reactive portion (channel) in response to the task.

Subsequently, the signal processing portion 30 correlates the calculated representative signals 601 10 and 602 with general hemoglobin variation signals obtained in response to a given task, in that a language stimulation and extracts a task related signal (step 205). The general hemoglobin variation signal pattern with respect to the task is one determined empirically 15 and experimentally by making use of other modalities in the field of medical imaging diagnosis such as an MRI apparatus and a PET apparatus, and it is known, for example, that the hemoglobin variation in response to a language stimulation shows a trapezoidal pattern, in 20 that rises in about 10 sec. from the start of the stimulation and decreases in about 10 sec. after ending the stimulation. When a task application pattern is fixed, these hemoglobin signal variation patterns can be stored beforehand in the memory portion 32, however, 25 in the present embodiment, a case will be explained in which a user prepares a hemoglobin variation signal pattern with respect to a task in response to any

application patterns to be set.

The preparation of the hemoglobin variation signal pattern is executed at the same time when, for example, by clicking "Reference Graph" button on the screen shown 5 in Fig.6, the displayed image as shown in Fig.6 is changed over to the one shown in Fig.7 (step 204). Fig.7 shows an example of screen images when a user prepares a language reference and response waveform 701, which is a general hemoglobin variation signal pattern with 10 respect to language stimulation. In this screen image, a box 705 is provided for inputting a delay time from the stimulation start to the appearance of the maximum value of the hemoglobin variation and from the stimulation end to the return of the hemoglobin 15 variation to the original state before the stimulation start, and when a delay time in response to a load is input in the box 705, a trapezoidal waveform having the delay time being input of, for example, 10 sec. is produced as the language reference and response 20 waveform 701 with respect to a rectangular waveform having a signal value 1 at the stimulation start point 702 and the stimulation end point 703. Then, the language reference and response waveform 701 thus produced is displayed by overlapping on the graph of 25 the representative signals 601~603 as shown in Fig.6 (In Fig.6, the language reference and response waveform is indicated as 605). Further, in the present embodiment,

although an example of inputting a numerical value for the delay time has been shown, in another example, while assuming the rectangular waveform having signal value of 1 at the stimulation start point 702 and at the 5 stimulation end point 703 as a figure, the delay time can be input by moving the two apexes of the rectangular in the direction of the time axis by dragging operation of a mouse. Further, since it is sufficient if the step 204 of preparing the language reference and response 10 waveform is executed prior to the step of calculating the correlation with the representative signals, the preparation step can be performed either before the start of the measurement or after the measurement.

The calculation result of the correlation between 15 the representative signals 601~603 and the language reference and response waveform 701, namely, the correlation value is displayed together with the graph of the representative signals. In the display example as shown in Fig.6, the correlation values are displayed 20 at the right end portions of the graphs of the representative signals as 611, 612 and 613. When observing the display result, the correlation value between the representative signal 601 and the language reference and response waveform 701 shows as 0.88 and 25 the correlation value between the representative signal 602 and the language reference and response waveform 701 shows as 0.14, therefore, it is understood that

among the two representative signals the representative signal 601 having a higher correlation value is the language related signal. Further, in this instance, in order to facilitate recognition that the representative 5 signal 601 is the language related signal, it can be possible after the correlation value calculation to change the color of the representative signal 601 having the highest correlation value, for example, in red and to display the same. Thereby a user can recognize at 10 a glance the language related signal.

As has been already explained above, on the screen showing the representative signals 601, 602 and 603, for the respective representative signals, the calculation results of the weights of every channel are displayed 15 in bar graphs. Accordingly, after observing the weights for the respective channels corresponding to the representative signal 601 serving as the language related signal, the operator specifies a channel having the highest weight (step 206). The channel having the 20 highest weight corresponds to an active portion in the brain where responds most to the language task. In the illustrated example, it is understood that the eighth channel shows the highest weight. Thereby, it is diagnosed that the active portion in the brain where 25 responds most to the language task is at a position of the eighth channel on the left temporal lobe. With regard to the bar graph display of the weights, it is

also possible to facilitate recognition if the color of the channel having the highest weight in bar graph is changed from that of the other channels, for example, the channel having the highest weight in bar graph is 5 colored in red, alternatively, only the channel having the highest weight in bar graph is displayed by inverting black and white. Further, it will be preferable to display an image showing an attachment state of the probe as shown in Fig.3 in a window and 10 to apply to the concerned channel the above referred to recognizable indication. Still further, these easy recognizable indications can be realized by softwares assembled in the control portion 31.

According to the present embodiment as has been 15 explained, after being displayed the hemoglobin variation signals measured (after step 202), by clicking "Calc PCA" button displayed on the same screen, since the extraction of the representative signals, the display of the representative signals and the weights 20 and the display of the task related signal determined from correlation with the predetermined language reference and response signal are performed, through observing the weights of the respective channels for the task related signal, the active portion where 25 responds most to the task can easily identified.

Now, when identifying an active portion in the brain not being limited to the identification of the

language area region, it is sometimes necessary to know which is dominance right hemisphere or left hemisphere. The living body photometric apparatus according to the present embodiment can be provided with a function of 5 determining such hemispheric dominance.

A flowchart of determining the hemispheric dominance is shown in Fig.8, in which steps 801~805 are equivalent to the steps 201~205 in Fig.2. Namely, the probes are attached to the right and left temporal lobes 10 where the language area exists (step 801), while giving a task to a subject under a predetermined condition, hemoglobin variation signals of the respective channels are measured (step 802). Subsequently, the principal component analysis is performed for the hemoglobin 15 variation signals of the respective channels, the representative signals are calculated as well as inherent vector values of the respective channels calculated through the principal component analysis are displayed as weights (abundance frequency) of the 20 respective channels for the representative signals (step 803). Subsequently, for the representative signals calculated in step 803, like Fig.2 embodiment, a correlation with the task reference and response waveform (produced at step 804), which is a typical 25 response pattern to the task is calculated and the task related signal is extracted (step 805).

When the task related signal (a representative

signal having the highest correlation value calculated) is extracted in the above manner, average values of the weights of every right and left channels for the task related signals are determined. The average values thus 5 determined are displayed, for example, as shown in Fig. 6, in numerical values at the bottom of the bar graphs showing the weights of the respective channels (step 806). In the example as illustrated, the average value of the weights of the channels 1~12 in the left 10 hemisphere is 0.25 and the average value of the weights of the channels 1~12 in the right hemisphere is 0.125. Further, in the present example, although the average values of the weights of every channels are calculated, it is possible to calculate and display such as average 15 values of absolute value weights, average values of only positive symbol weights or negative symbol weights and average values of weights of above or below a predetermined threshold value.

The hemispheric dominance LI (Laterality Index) 20 of right and left brain activity can be calculated according to equation (1) by making use of the average values 614 and 615 of weights for right and left hemisphere.

$$LI = (Al - Ar) / (Al + Ar) \quad \cdots (1)$$

25 Wherein, Al is the average value of weights for the left hemisphere and Ar is the average value of the weights for the right hemisphere.

The above calculation according to equation (1) is performed either in the signal processing portion 30 or in the control portion (CPU) 31 by making use of a software assembled therein.

5 The hemispheric dominance LI thus determined, although not illustrated, is displayed, for example, at the center of bar graphs of right and left weights as shown in Fig.6 as "LI=0.33". This implies that $A_L > A_R$ in equation (1), namely, shows that the left 10 hemisphere is dominant, and 0.33 shows including "+" symbol. Oppositely, when $A_L < A_R$ in equation (1), it is indicated as "LI=-0.33" by adding "-" symbol to show that the right hemisphere is dominant. Further, the symbols "+" and "-" can be converted into letters "left" 15 and "right" through a software.

In the above explanation, the example in which the measurement was performed after attaching the probes to the right and left temporal lobes and dominance of either the right or left hemisphere was judged, however, 20 it is also possible to further divide the brain active region and to measure the same and then to judge their dominance. Further, in the above explanation, although the identification of language area region was primarily explained, it is also possible to identify 25 regions other than the language area, such as to identify a visual area by giving a subject a visible stimulation as a task.

According to the present invention as has been explained hitherto, through extracting from the measured data only the activity signals in the brain caused by the task (task related signal) and by 5 specifying a channel having the highest correlation with the signal, thereby, the active portion in the brain where responds most to the task can be identified.

Further, according to the present invention, through displaying such as the task related signals and 10 the abundance frequency in the respective channels for the task related signals, a user can easily identify visually the active portion in the brain.

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